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**Biomechanical metrics of aesthetic perception in dance**

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**Abstract**

The brain may be tuned to evaluate aesthetic perception through perceptual chunking when we observe the grace of the dancer. We modelled biomechanical metrics to explain biological determinants of aesthetic perception in dance. Eighteen expert (EXP) and intermediate (INT) dancers performed *développé arabesque* in three conditions: i) slow tempo, ii) slow tempo with relevé, and iii) fast tempo. To compare organizational metrics of kinematic data, we calculated intra-excursion variability, principal component analysis (PCA), and dimensionless jerk for the gesture limb. Observers, all trained dancers, viewed motion capture stick figures of the trials and ranked each for i) aesthetic proficiency and ii) movement smoothness. Statistical analyses included group by condition repeated measures ANOVA for metric data; Mann-Whitney U rank and Friedman’s rank tests for non-parametric rank data; Spearman’s rho correlations to compare aesthetic rankings and metrics; and linear regression to examine which metric best quantified observers’ aesthetic rankings,  $p < 0.05$ . The goodness of fit of the proposed models were determined using Akaike Information Criteria (AIC). Aesthetic and smoothness rankings of the dance movements revealed differences between groups and condition,  $p < 0.0001$ . EXP were rated more aesthetically proficient than INT dancers. The slow and fast conditions were judged more aesthetically proficient than slow with relevé ( $p < 0.0001$ ). Of the metrics, PCA best captured the differences due to group and condition. PCA also provided the most parsimonious model to explain aesthetic rankings. By permitting organization of large data sets into simpler groupings, PCA may mirror the phenomenon of chunking in which the brain combines sensory-motor elements into integrated units of behavior. In this representation the chunk of information which is remembered, and to which the observer reacts, is the elemental mode shape of the motion rather than physical displacements. This suggests that reduction of redundant information to a simplistic dimensionality is related to the experienced observer’s aesthetic perception.

**Key words:** Akaike Information Criteria, chunking, dimensionless jerk, principal component analysis, variability

51  
52 **INTRODUCTION**

53           In 1623, the astronomer Galileo Galilei observed that the universe "is written in the  
54 language of mathematics" (Tegmark, 2008). More recently, Max Tegmark wrote "our external  
55 physical reality is a mathematical structure" (Tegmark, 2008). Perception of dance (visual) or  
56 music (auditory) is perception of reoccurring shapes and patterns. These shapes and patterns,  
57 in the abstract, are based on numerical relationships, which are expressions of space and time.  
58 In movement analysis, we employ biomechanical mathematics to describe and analyze  
59 movement. Here, we ask, is there an biomechanical metric that relates to our aesthetic  
60 perception of the dancer?

61  
62 *Aesthetic perception*

63           When two dancers perform the same movement, a movement practiced multiple times  
64 on a daily basis, how does the viewer intuitively know that one dancer embodies greater  
65 aesthetic proficiency or is more pleasing (Calvo-Merino, Ehrenberg, Leung, & Haggard, 2010;  
66 Calvo-Merino, Jola, Glaser, & Haggard, 2008; E. S. Cross, Kirsch, Ticini, & Schutz-Bosbach,  
67 2011)? Dance (and music) has been a medium for communities to interrelate since primitive  
68 societies (I. Cross, 2012; Kraus, Hilsendager, & Gottschild, 1991). As dance moved to the  
69 performance venue, it became removed from group communal interaction to one of observer –  
70 performer or audience and dancers. This assumes there are aesthetic properties to dance  
71 movement and that the audience experiences an aesthetic response of some sort (Bläsing et  
72 al., 2012). Depending upon their movement experience, observers may evaluate their aesthetic  
73 experience in several ways; through cognitive judgement or affective appreciation (valence) of  
74 dance movement based upon qualities such as movement amplitude, velocity, difficulty, or  
75 control; while others may include their own familiarity and physical ability in their aesthetic  
76 appreciation (Chatterjee, 2003; E. S. Cross, Kirsch, Ticini, & Schütz-Bosbach, 2011; Leder,  
77 Belke, Oeberst, & Augustin, 2004; Montero, 2012; Torrents, Castaner, Jofre, Morey, & Reverter,  
78 2013). The information-processing model presented by Leder et al. (2004) suggests that there  
79 are two types of output in aesthetic processing: aesthetic emotion and aesthetic judgement  
80 (Leder et al., 2004). To date, the majority of research on dance aesthetics has focused on  
81 emotional liking: the observers' perception of affect and affective response to dance (Calvo-  
82 Merino et al., 2008; Christensen, Nadal, & Cela-Conde, 2014; Kirsch, Drommelschmidt, &  
83 Cross, 2013; Orgs, Hagura, & Haggard, 2013). The cognitive aesthetic evaluation of technical  
84 proficiency such as control, accuracy, and fluidity, the focus of this study, has been less studied.

85           With no external goal to quantify a score, can we quantify the difference in the viewer's  
86 aesthetic judgement of these two dancers performing the same movement? What is the  
87 relationship between this perception of dance, in this case a ballet sequence, and its  
88 biomechanical organization? Does the observer perceive dance movement with some  
89 organizational strategy for recall? Does the concept of chunking for the purpose of extracting  
90 meaningful event features, while suppressing extraneous information, relate to a kinematic  
91 metric?

92

### 93 *Linear and nonlinear metrics in human movement*

94           A dynamic systems approach offers determination of coordinative patterns that may be  
95 overlooked in more traditional linear kinematic measures organized around measures of  
96 centrality. Movement patterns in high and low skilled subjects or those with dysfunction can be  
97 considered adaptations to the constraints of mechanics, environment, and task. Most  
98 movements, such as walking, display stereotypical spatial-temporal patterns, which suggests  
99 that human movements organize degrees of freedom into functional coupled relationships to  
100 achieve the task. These constraints, resulting from what are apparently complex motions,  
101 consist of significantly less active degrees of freedom than an unconstrained system. These  
102 degrees of freedom are patterns of joint movements rather than individual articulations.  
103 Because motor behavior is also inherently variable, the challenge is to identify coordination  
104 patterns that may distinguish different groups of subjects, with greater skill or disability, or  
105 between conditions of differing levels of difficulty. A widely applied method in structural  
106 dynamics is to describe complicated movements in terms of a small number of underlying  
107 modes of vibration (e.g. principal component analysis). Could principal component analysis  
108 (PCA) also be related to the manner in which elements are chunked into larger combinations as  
109 as part of the aesthetic perception of movement?

110           Coordination variability can be assessed by approaches such as angle-angle plots, PCA,  
111 vector coding, and entropy. Seemingly contradictory research findings suggests that there is an  
112 'optimal' coordination variability in healthy, skilled subjects, no matter what the movement, that  
113 is necessary to permit adaptation to mechanical, environmental, and task constraints (Chow,  
114 Davids, Button, & Koh, 2008; Pollard, Heiderscheit, van Emmerik, & Hamill, 2005; Stergiou &  
115 Decker, 2011; Wagner, Pfusterschmied, Klous, von Duvillard, & Muller, 2012). This lies between  
116 the higher and lower variability reported in populations with less skill or neurologic and  
117 musculoskeletal dysfunction (Hamill, van Emmerik, Heiderscheit, & Li, 1999; Hein et al., 2012;

118 Kiefer et al., 2013). The majority of analyses, to date, have focused on sports activities that  
119 have an end goal such as speed or accuracy.

120         Patterns of variability (e.g. simple v. complex skills, injured v. healthy subjects) may not  
121 be generalizable and may differ depending on the movement to be analyzed (e.g. basketball  
122 dunk v. ballet movement). To date, dynamic systems approaches have been applied to the  
123 analyses of dance movements in only limited fashion (Hollands, Wing, & Daffertshofer, 2004;  
124 Reeve, Hopper, Elliott, & Ackland, 2013; Smith, Siemienski, Popovich, & Kulig, 2012; Torrents  
125 et al., 2013; Vincs & Barbour, 2014). Are certain metrics sensitive to determine differences due  
126 to skill level or condition difficulty in ballet movement?

127         Maximum smoothness theory introduced the jerk metric, the third time derivative of  
128 position, as a quantitative principle of motor control as well as a way to characterize the smooth  
129 gracefulness of natural movements (Hogan & Flash, 1987). This brings dance immediately to  
130 mind. A number of jerk measures have been used to quantify smoothness and coordination in  
131 studies that examine changes due to neurologic impairment and rehabilitation (Rohrer et al.,  
132 2002; Teulings, Contreras-Vidal, Stelmach, & Adler, 1997; Yan & Dick, 2006). It has been used  
133 less frequently to examine differences in skill level (Hreljac, 1993). Jerk may provide a metric for  
134 the objective quantification of smoothness of motion and, by extension, to the skill level of the  
135 practitioner. Recently, Hogan and Sternad (Hogan & Sternad, 2009) described the inability of  
136 numerous measures of jerk to correlate with a *subjective* assessment of smoothness of  
137 movement. These jerk measures, depending on their individual formulation, had dimensions of  
138 time and position to appropriate powers. They proposed a dimensionless measure of jerk which  
139 was found to be insensitive to periods of inactivity and more accurately reflected divergence  
140 from smooth and coordinated movement. Does dimensionless jerk correlate with subjective  
141 smoothness when assessed by trained dance observers?

142

### 143 *Aesthetic criterion of dance*

144         In ballet, the goal of movement is to meet an technical aesthetic criterion, that includes  
145 specific timing and spatial relationships of upper and lower extremity placement, while making it  
146 appear effortless (Autere, 2013; Cohen, 1997; Hagendoorn 2005). Previous researchers,  
147 examining frequently performed ballet movements such as the *développé arabesque* and *grand*  
148 *rond de jambe en l'air*, reported similar movement organization and timing across various levels  
149 of expertise (e.g. expert, advanced, and intermediate dancers) (Bronner, 2012; Kwon, Wilson,  
150 & Ryu, 2007; M. Wilson, Lim, & Kim, 2004). In these studies there were no differences in limb  
151 angular displacement and velocity. Only kinematic control of the pelvis (e.g. three-dimensional

152 (3-D) peak angular displacement) appeared to differentiate skill level. However, the prescribed  
153 timing and spatial directives may have constrained these biomechanics findings. If there is no  
154 difference between the two dancers in the general shape and timing kinematics of the dance  
155 movement (e.g. peak angular displacement and velocity), alternative approaches are called for.  
156 Could this be due to stability (e.g. less variability), a cost function, or some other set of  
157 kinematic parameters such as dimensionless jerk or nonlinear variability algorithms such as  
158 principal component analysis? Furthermore, does differentiation of skill and condition by a  
159 kinematic metric relate to observer perception?

160 The purpose of this study was three-fold. The first aim was to apply linear and nonlinear  
161 dynamic systems approaches to determine the sensitivity of these metrics to differentiate skill  
162 level and condition in a complex ballet sequence, the *développé arabesque*. The second aim  
163 was to determine whether experienced observer rankings of the performers' *développé*  
164 *arabesque*, viewing abstracted motion capture stick figures, for technical aesthetic proficiency  
165 and movement smoothness can also differentiate skill level and condition. Finally, the third aim  
166 was to compare these biomechanical metrics to the experienced observer rankings for  
167 aesthetics and smoothness to determine which metric best quantified observer perceptions of  
168 the dancers' *développé arabesque* sequence.

169

## 170 2. METHODS

### 171 *Subjects*

#### 172 Dancers

173 Eighteen healthy adult dancers (12 female, 8 male), recruited from internationally  
174 recognized professional dance companies and affiliated pre-professional training programs,  
175 volunteered for this study. Each dancer was assigned to one of two groups with distinct levels of  
176 dance expertise: i) expert and ii) intermediate. The expert (EXP) group was based on  
177 employment in a professional company. The intermediate (INT) group, comprised of student  
178 dancers, was determined by ballet class placement by dance faculty. During auditions, students  
179 are placed into ballet technique classes that ranged from beginning to advanced levels (Ballet 1-  
180 7); we selected students placed into Ballet 4 and 5, or intermediate level classes. Inclusion  
181 criteria was the ability to attain the criterion dance sequence, *développé arabesque*, at a height  
182 of 90° (e.g. gesture limb perpendicular to the stance limb and parallel to the floor) and exclusion  
183 was a history of lower extremity injury during the previous six months that caused a dancer to  
184 stop dancing for one week or more. We did not include naïve or beginner participants in this  
185 study because naïve and beginner dancers were not able to meet the inclusion criteria. The

186 university Institutional Review Board approved this study. A power analysis of sample size for a  
187 two group repeated measures with three conditions (2 X 3) study, with a large effect size  
188 ( $f=0.80$ ),  $power=0.95$ , and  $\alpha = 0.05$ , determined a sample size of 8 was necessary. Therefore,  
189 the selected sample size of 18 subjects was more than sufficient. Participant demographics  
190 were collected at intake.

191 The ratio of female to male dancers was the same within each group (5 females, 4  
192 males). Comparison of group demographics was performed using a paired t-test for  
193 independent samples. There were differences between groups in age (EXP =  $25.8 \pm 2.6$  and  
194 INT =  $20.4 \pm 1.5$  years,  $p<0.0001$ ) and years of dance experience (EXP =  $15.22 \pm 6.68$  and INT  
195 =  $5.50 \pm 5.15$  years,  $p=0.003$ ), but no difference in height ( $1.71 \pm 0.076$  m), mass ( $62.20 \pm 8.67$   
196 kg), leg length ( $0.92 \pm 0.05$  m), or starting first position turnout ( $107.94 \pm 11.89^\circ$ ).

197

### 198 Observers

199 Previous research has reported differences in the aesthetic experience of viewers with  
200 differing levels of expertise in performing the observed movements (Calvo-Merino et al., 2010;  
201 E. S. Cross, Kirsch, Ticini, & Schutz-Bosbach, 2011; Kirsch et al., 2013). Therefore, we selected  
202 trained dancers to act as observers of the arabesque sequences. Experienced dancers are able  
203 to rapidly process movement, developed as part of their training, and may use 'schematic  
204 expectancies' to maximize their short-term memory (C. Stevens et al., 2010). Twenty seven  
205 different dancers, recruited from international caliber professional dance companies and  
206 affiliated pre-professional training programs, volunteered to evaluate the arabesque data for i)  
207 aesthetic proficiency and ii) smoothness. Observers included nine professional and 18  
208 advanced or intermediate pre-professional dancers (22 female, 5 male), They had a broad span  
209 of dance experience from 4 to 40 (mean  $15 \pm 9$  years and ranged from 18 to 55 (mean  $28 \pm 12$ )  
210 years of age.

211

### 212 *Experimental Protocol*

#### 213 Motion capture

214 The dance-specific task, *développé arabesque*, was a sequential, multi-joint movement  
215 that required intra and inter-segmental coordination of lower and upper extremity movement  
216 with changes from bipedal to unipedal postural control. It is practiced in every ballet class, and  
217 consequently was well known to each subject. Each dancer's preferred *1<sup>st</sup> position* foot  
218 placement (heels touching with lower extremities externally rotated) was marked on the floor,  
219 measured (Bronner, 2012), and used as the starting position (Fig. 1).

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Insert Fig. 1 here

A tape recording of a metronome with voice instruction overlay provided the tempo of the movement sequence (40 or 90 beats·min<sup>-1</sup>). Dancers practiced the *développé arabesque* sequence (Fig. 1A – D) for three conditions prior to data acquisition to synchronize their movements with the metronome. The dancers were instructed to emphasize spatial and temporal precision. From the starting posture (1<sup>st</sup> position), the gesture lower extremity passed through *passé* (hip and knee flexion, with ankle plantar flexion), and extended posteriorly to *arabesque* (gesture hip and knee extension with ankle plantar flexion), where it was held for one count, followed by return to the initial *1<sup>st</sup> position*. Dancers performed six consecutive ‘excursions’ (or repetitions of the *développé arabesque sequence*) within one trial with the right lower extremity as gesture limb. This was followed by six consecutive ‘excursions’ with the left lower extremity as gesture limb.

The *développé arabesque* sequence was performed in three conditions to reflect differing tempo and balance constraints. For Condition 1, the *développé arabesque* was performed on flat foot at a tempo of 40 beats·min<sup>-1</sup> (Slow-flat). For Condition 2 using the same 40 beats·min<sup>-1</sup> tempo, dancers were asked to *relevé* (rise up onto the toes of the stance limb and hold) (Slow-bal) during the arabesque phase of the sequence. For Condition 3, the *développé arabesque* was performed on flat foot at a tempo of 90 beats·min<sup>-1</sup> (Fast). The excursions lasted approximately 40s in length for Conditions 1 and 2, and 18s for Condition 3.

Kinematic data were collected at a sampling rate of 120 Hz, with a 5-camera motion analysis system (Vicon 250, Oxford Metrics Ltd, Oxford, UK). A full body marker set comprised of 29 reflective, spherical markers in the Plug-In gait marker set was used to create an 11-segment model. Attire for all subjects consisted of a dark colored unitard to maximize contrast of reflective markers.

Kinematic data were reconstructed using a Vicon Bodybuilder model (Oxford Metrics Ltd, Oxford, UK). Kinematic data were filtered with a 4th order 20Hz order low pass FIR filter. Dance movements may require movement of three or more limbs; four in the case of a jeté or leap. Both upper extremities and one lower extremity are moving in the *développé arabesque*. In ballet, the gestural foot is often considered an expressive focal point. Therefore, we focused our analysis on the gestural lower extremity.

### Observer rankings



254 We defined *aesthetic proficiency* as the technical accuracy of timing, dynamics, and  
255 shape as performed by each dancer. We defined *smoothness* as the fluid trajectory of the lower  
256 extremity gesture limb. The ranking numbers 1-18 were selected for the total number of  
257 subjects, with 1 for most to 18 for least in: i) aesthetic technical proficiency, and ii) movement  
258 smoothness. Aesthetic proficiency and smoothness rankings were conducted in separate  
259 sessions. Ranking was selected, rather than rating, in order to compare each dancer to the  
260 others within a given condition. Observers evaluated the abstracted motion capture stick figure  
261 data for the left and right lower extremity as gesture limb of all subjects on a laptop computer  
262 within one condition in a single viewing (add youtube movie example of stick figures). Group  
263 assignment was unknown to the observers. There were six consecutive 'excursions' within one  
264 trial per gesture limb. Observers were permitted to view a trial again if needed as they  
265 reorganized the ranking numbers of a given condition.

266

## 267 *Data analysis*

### 268 Observer rankings

269 Mean aesthetic and smoothness observer rankings were calculated for each dancer trial  
270 in each condition. For the aesthetic and smoothness rank data, the non-parametric Mann-  
271 Whitney U rank test for two independent samples was used to determine group differences. The  
272 non-parametric Friedman two-way ANOVA rank test (K-related samples) was used to determine  
273 condition differences. Statistical significance was set at  $p \leq 0.05$  for both the Mann-Whitney and  
274 Friedman tests. If significance was determined in the Friedman test, post hoc pairwise  
275 comparisons were conducted using the Wilcoxon signed-rank test with a Bonferroni correction  
276 ( $0.05/3 = 0.017$ ). The assumption of homogeneity of variance was checked for aesthetic and  
277 smoothness rank data using Levene's test for non-parametric ranked data.

278

### 279 Three-D pelvis-hip angle-angle and toe displacement variability

280 Intra-excursion variability for the pelvis-hip, an important control area (Bronner, 2012),  
281 was calculated on the angle-angle phase plane for all three cardinal planes. For the 3-D angle-  
282 angle analysis, pelvis inclination was defined as the included angle between the normal to the  
283 right anterior iliac spine (RASIS), left anterior iliac spine (LASIS), sacrum plane and global  
284 vertical. The hip articulation angle was defined as the included angle between the femur  
285 proximal to distal axis and the normal to the RASIS, LASIS, sacrum plane. Each trial was  
286 decomposed into its constituent excursions (six per trial). The excursion commenced when the

287 toe marker on the gesture leg exceeded an altitude of 190mm and ended when the marker  
288 descended below 190mm.

289 The 3-D angle of the pelvis and hip angle between the normal of the pelvis and  
290 the proximal/distal axis of the gesture femur were calculated. The standard deviation  
291 across the excursions of the pelvis and hip angles were calculated as a fractional basis  
292 of the excursions. The pelvis-hip MSD was the mean of these standard deviations.

293 We did not normalize the temporal component of the data of these excursions as this  
294 process can distort the spatial relationship between trials (Hamill, McDermott, & Haddad, 2000),  
295 which was a parameter of interest. Furthermore, dancers have been found to be extremely  
296 consistent when performing movements to an external tempo (Reeve et al., 2013).

297 Three-D angle-angle plots were constructed of the pelvis and hip for the  
298 three conditions and an MSD value was calculated for each subject. Similarly, MSD was  
299 calculated for the 3-D toe displacement using the same decomposition into its constituent  
300 excursions (six per trial) and onset and offset criteria. The mean and standard deviation of the  
301 gesture toe was calculated along its 3-D trajectory. The toe MSD was the mean of the standard  
302 deviation along the trajectory.

303 Because each excursion had a discrete onset and offset, circular statistics were not  
304 necessary. To compare pelvis-hip and toe variability for left and right gesture limbs, separate 2  
305 (group) X 3 (condition) repeated measures ANOVA comparisons were conducted, with pairwise  
306 comparisons. Statistical significance was set at  $p \leq 0.05$  for all tests.

307

### 308 Principal component analysis

309 PCA is a data reduction technique for the compression of large data sets (Jolliffe, 2002)  
310 and has been shown to be appropriate for feature extraction in human movement analysis  
311 (Daffertshofer, Lamoth, Meijer, & Beek, 2004). PCA was used to quantify 3-D kinematic patterns  
312 using the full data set. The joint angle time histories were calculated from the motion data. A 15-  
313 element state vector was defined for each time instant of each trial from the angular position of  
314 the pelvis (3 degrees of freedom (DOF) in a rotation sequence about the P-A axis, followed by  
315 rotation about the lateral axis, followed by rotation about the S-I axis) together with the joint  
316 articulations of the hip (3 DOF in a rotation sequence about the abduction/adduction axis,  
317 followed by rotation about the flexion/extension axis, followed by rotation about the  
318 internal/external rotation axis), knee flexion (1 DOF) and ankle dorsi/plantar flexion and  
319 internal/external rotation (2 DOF) of the stance and gesture limbs. Knee flexion was defined as  
320 the angle between the line from the knee joint centre to the hip joint centre and the line from the

321 knee joint centre to the ankle joint centre in the plane defined by these two lines. These  
322 variables were selected as elements in the state vector as they span the domain of possible  
323 lower limb motion with the exception of knee varus/valgus and ankle abduction/adduction which  
324 were considered trivial.

325 The principal components were calculated for the matrix of the above vector for each  
326 time in the trial. The matrix was initialized normalized, so that they have zero mean and unity  
327 variance. Principal components that contributed less than 2% to the total variance in the data  
328 set were eliminated. Mean dimensionality of the non-redundant state manifold count was  
329 calculated for each group and condition and compared with a 2 X 3 repeated measures  
330 ANOVA, with pairwise comparisons,  $p \leq 0.05$ .

331

### 332 Jerk

333 Dimensionless jerk as described by Hogan and Sternad (2009), was calculated for 3-D  
334 linear displacement of the gesture toe as:

335

336  $\text{Jerk}_{\text{dimensionless}}$

$$= \frac{D^3 \int_{t_1}^{t_2} \ddot{x}(t)^2 dt}{V_{\text{mean}}^2}$$

337

338 where  $D$  = duration of the trial

339  $x(t)$  = position variable

340  $v$  = first time derivative of the position variable

341

342 and for 3-D angular displacement of the gesture hip as:

343

344  $\text{Jerk}_{\text{dimensionless}} =$

$$D^5 \int_{t_1}^{t_2} \ddot{\theta}^2 dt$$

345

346 where  $\theta$  = angular displacement

347

348 Separate 2 (group) X 3 (condition) repeated measures ANOVA comparisons for the i) 3-D linear  
 349 displacement of the gesture toe; and ii) 3-D angular displacement of the gesture hip were  
 350 conducted, with pairwise comparisons. Statistical significance was set at the  $p \leq 0.05$  for all tests.

351

352 Correlation of observer rankings and biomechanical variables

353 Aesthetic rankings were compared to smoothness rankings, MSD for 3-D pelvis-hip  
 354 angle-angle and toe displacement variability, PCA, and dimensionless jerk for 3-D hip angle and  
 355 toe displacement using Spearman's rho correlations for nonparametric variables,  $p \leq 0.05$ .

356

357 Modeling rankings and movement metrics

358 We employed mixed model linear regression analysis to examine which variables, MSD,  
 359 PCA, and jerk, were good predictors of each observer's aesthetic and smoothness perception.  
 360 Separate regression analyses approximated the i) aesthetic; and ii) smoothness ranking data  
 361 with regressors that consisted of the following:

362 Model 1) 5 predictors: PCA, jerk (hip and toe), and MSD (3-D pelvis-hip and toe);

363 Model 2) 1 predictor: PCA;

364 Model 3) 2 predictors: jerk (hip and toe);

365 Model 4) 1 predictor: toe jerk;

366 Model 5) 2 predictors: MSD (pelvis-hip and toe); and

367 Model 6) 1 predictor: MSD toe.

368

369 The goodness of fit of the proposed models were determined using Akaike Information Criteria  
 370 (AIC), with the least AIC value, indicating the best fit. The AIC value is

371

372

$$AIC = 2k - 2 \ln(L),$$

373

374 Where  $k$  is the number of parameters in the model, and  $L$  is the maximized likelihood function  
375 for the model. The corrected AIC value (AICc) for finite sample size where

376

$$377 \text{AICc} = \text{AIC} + 2k(k+1)/(n-k-1)$$

378

379 was selected for comparison of the models. All statistics were conducted using SPSS (SPSS v.  
380 21, IBM Corp, Armonk, NY).

381

## 382 **RESULTS**

### 383 *Observer rankings*

384 The Mann-Whitney U test for group indicated that aesthetic rankings were lower for EXP  
385 dancers (median = 4.10, interquartile range (IQR) = 2.20-6.20) compared to INT dancers  
386 (median = 10.20, IQR = 8.20-12.00) [U=88.00,  $p < 0.0001$ ]. A non-parametric Friedman test of  
387 differences among repeated measures for condition was conducted, rendering a Chi-square test  
388 value of 15.267,  $p < 0.0001$ . Post hoc Wilcoxon signed-rank test indicated that Slow-flat aesthetic  
389 rankings (median = 7.75, IQR = 4.88-10.13) were significantly lower than Slow-bal (median =  
390 8.30, IQR = 5.17-12.00) [ $z = 2.109$ ,  $p = 0.017$ ]; Fast rankings (median = 7.90, IQR = 2.20-11.20)  
391 were also lower than Slow-bal [ $z = 3.570$ ,  $p < 0.0001$ ]; and Slow-flat was lower than Fast [ $z =$   
392 2.233,  $p = 0.012$ ]. [Note, lower rank indicated greater excellence in aesthetic proficiency  
393 rankings. For smoothness results see Supplement.]

394

395 Insert Fig. 2 here

396

### 397 *Three-D pelvis-hip angle-angle and toe displacement variability*

398 Three-D gesture limb pelvis-hip angle-angle plots for a representative subject from each  
399 group performing six excursions during each condition are seen in Fig. 3. The MSD seen in the  
400 six plots demonstrate variability around the mean. Comparisons found a significant difference  
401 between groups [ $F(34,1) = 6.532$ ,  $p = 0.015$ ] (Fig. 4A), with EXP displaying lower pelvis-hip angle-  
402 angle MSD than INT dancers. There were no differences between conditions.

403 There were group differences in 3-D toe displacement MSD [ $F(34,1) = 12.406$ ,  $p = 0.001$ ]  
404 with EXP reflecting lower toe MSD than INT, and for condition [ $F(34,1) = 5.277$ ,  $p = 0.028$ ]. Fast  
405 condition 3-D toe MSD was lower than the Slow-bal condition ( $p = 0.014$ ). There was an  
406 interaction between group and condition [ $F(34,1) = 4.254$ ,  $p = 0.047$ ] (Table 1, Fig. 4B). Three-D  
407 toe MSD was lower in EXP compared to INT dancers in the Slow-flat ( $p = 0.047$ ) and Slow-bal

408 conditions ( $p=0.004$ ).

409

410

Insert Figs. 3 and 4 here

411

412 *Principal component analysis*

413 The PCA analysis had three effects: (1) it orthogonalized the components of the input  
414 vectors so that they were uncorrelated with each other; (2) it ordered the resulting orthogonal  
415 components (principal components) so that those with the largest variation came first; and (3) it  
416 eliminated those components that contributed the least to the variation in the data set. The PCA  
417 dimensionality of the movement reported indicates the number of mode shapes which were  
418 required to account for 98% of the total variance of the motion data captured during the  
419 arabesque excursions.

420 Figure 5A shows an example of five principal modes calculated for a representative INT  
421 dancer. The first mode, and hence the mode contributing the most variance to the movement,  
422 was predominantly a hip flexion/extension motion. The second mode was mainly a hip  
423 abduction/adduction. The third mode was associated with knee flexion/extension of the support  
424 limb, the fourth mode was support limb ankle internal/external rotation, and the fifth mode was  
425 associated with gesture limb ankle internal/external rotation. The combination of these five  
426 modes accounted for 98% of the variance of the trial.

427

428

Insert Fig. 5 here

429

430 Figure 5B shows an example of the four principal modes calculated for a representative  
431 EXP dancer. The first mode consists of hip flexion/extension motion, similar to the intermediate  
432 dancer. The second mode for the expert dancer was also mainly a hip abduction/adduction,  
433 however the third mode was dominated by support limb ankle internal/external rotation. The  
434 fourth mode was primarily support limb knee flexion/extension. These four modes accounted for  
435 98% of the variance of the trial.

436 The mean dimensionality of the state manifold accounting for 98% of the variance for  
437 EXP dancers was significantly lower than the mean dimensionality for INT dancers for group  
438 [ $F(34,1)=25.339$ ,  $p<0.0001$ ] and condition [ $F(34,1)=14.876$ ,  $p<0.0001$ ] (Fig.6A and B). Post hoc  
439 pairwise comparisons for condition indicated there were differences between Slow-bal and  
440 Slow-flat ( $p=0.008$ ) as well as Slow-bal and Fast ( $p<0.0001$ ), with Slow-flat and Fast less than  
441 Slow-bal.

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Insert Fig. 6 here

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445 *Dimensionless jerk*

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Insert Fig. 7 here

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455 *Relationships between aesthetics and biomechanical variables*

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462 *Modeling rankings and movement metrics*

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Insert Table 1 here

467

## 468 **DISCUSSION**

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In general, observer aesthetic and smoothness rankings and biomechanical parameters were capable of distinguishing between group and condition, with the exception of 3-D toe jerk and pelvis-hip angle-angle MSD metrics. In discrimination between groups, kinematic metrics revealed that the movement of EXP dancers was smoother (e.g. lower jerk), more consistent (e.g. lower MSD), and displayed lower organizational parameters (fewer principal components) across all conditions. Differences between groups were generally greater in the Slow-flat and Slow-bal conditions compared to the Fast condition. In discerning differences between

476 conditions for both groups, there was generally an inverted horseshoe trendline to the data, with  
477 Slow-bal reflecting higher rankings for aesthetics (e.g. less aesthetic proficiency) and  
478 smoothness (e.g. less smooth), higher MSD, higher dimensional components, and higher jerk.  
479 In contrast, the Fast condition reflected the lowest number of principal components and lowest  
480 jerk. PCA provided the most parsimonious model to explain observer rankings. Each of the  
481 variables are discussed further in the sections below.

482

### 483 *Observer rankings*

484 We chose dancer-observers who were well trained in the movements that they ranked  
485 for aesthetics and smoothness. Evidence suggests that cortical regions involved in the action-  
486 observation network respond more strongly when the observer sees a kinesthetically familiar  
487 movement compared to one that the observer has never performed (Bläsing et al., 2012; Calvo-  
488 Merino, Glaser, Grezes, Passingham, & Haggard, 2005; E. S. Cross, Hamilton, & Grafton,  
489 2006). Aesthetic judgement has been linked to both action and processing fluency (Hayes, Paul,  
490 Beuger, & Tipper, 2008; Reber, Schwarz, & Winkielman, 2004). Experienced dancers compared  
491 to naïve observers judge the motor perceptual experience of precision, fluidity, and control  
492 differently. Therefore, we selected dancers to perform the observer rankings with the  
493 expectation that this expertise refines their observation of the technical aesthetic qualities of  
494 dance (Montero, 2012). In this study, despite reviewing the motion capture stick figures on  
495 separate occasions to rank for aesthetic proficiency or smoothness, rankings for aesthetic  
496 proficiency and smoothness were highly correlated. This suggests that movement fluidity may  
497 be an important component of cognitive aesthetic perception.

498 Several groups have developed dance-specific aesthetic competence evaluation  
499 measures that focus on the cognitive aspects of aesthetics such as technique accuracy,  
500 dynamics, and control (Angioi, Metsios, Twitchett, Koutedakis, & Wyon, 2009; Chatfield &  
501 Byrnes, 1990; Krasnow & Chatfield, 2009). Each group demonstrated excellent repeatability  
502 between judges in their respective measures, with sensitivity to determine change with training  
503 or due to expertise. Similar judgement of competency is also used in sports competitions such  
504 as diving, gymnastics and figure skating (Díaz-Pereira, Gómez-Conde, Escalona, & Olivieri,  
505 2014; Looney, 2004; Pajek, Cuk, Pajek, Kovac, & Leskosek, 2013; Young & Reinkensmeyer,  
506 2014). We chose to rank aesthetic judgement specific to each dancer's ballet technique for this  
507 reason. Aesthetic valience may be more variable across individuals due to personal taste (Leder  
508 et al., 2004).

509 Researchers have employed several ways of displaying dance movement in order to



510 study the aesthetic perception of dance. Observers have viewed dance as point light displays  
511 (Sevdalis & Keller, 2011), motion capture stick figures (Sato, Nunome, & Ikegami, 2014;  
512 Torrents et al., 2013), static stick figures (Daprati, Iosa, & Haggard, 2009), video (Calvo-Merino  
513 et al., 2008; E. S. Cross, Kirsch, Ticini, & Schütz-Bosbach, 2011; Jola & Grosbras, 2013; Miura  
514 et al., 2010), and live performance (Angioi et al., 2009; Stevens et al., 2009). Observation of live  
515 and video performances are most ecologically valid and may be important to study aesthetic  
516 valence. In contrast, abstraction of the dancer's movement in point-light or motion capture stick  
517 figure representation allows the observer to focus on form and fluidity to make technical  
518 aesthetic judgements without distraction by costumes, sets, or music.

519 Observers were able to distinguish between groups and conditions with both aesthetic  
520 proficiency and smoothness rankings. It is possible that these dancer-observers were able to  
521 accomplish this due to their specialized training in recognizing movement configurations,  
522 encoding them (in the case of ballet, this may include verbal encoding as it has a set  
523 vocabulary), and then extracting key information as part of the process of learning new  
524 choreography (C. Stevens et al., 2010; Stevens, Ginsborg, & Lester, 2010). In this study, the  
525 *développé arabesque* was a relatively short, well-learned phrase, enabling the observers to  
526 focus on differences between the performers.

527

#### 528 *Relationships between observer rankings and biomechanical variables*

529 Our results found that aesthetic rankings and all variables were significantly correlated.  
530 The highest correlation between aesthetic proficiency and biomechanical metrics was to PCA  
531 ( $r=0.620$ , greater than that of smoothness to PCA,  $r=0.479$ , see Supplement). Recently, multiple  
532 factor analysis (MFA), an extension of PCA to handle multiple data tables that measure sets of  
533 variables collected on the same observations, was applied to four dance movements: (1)  
534 *arabesque penchée* requiring balance; (2) *tour en dehors* or turn; (3) *brisé volé en arrière en*  
535 *tournant* or skater's jump; and (4) a forward fall, performed by expert dancers (Torrents et al.,  
536 2013). Non-expert observers rated motion capture stick figures performing each of the  
537 movements for aesthetic 'beauty.' Movement amplitude was the basic parameter used in  
538 judging positive aesthetics, followed by turning velocity, and the length of time that balance was  
539 maintained. In other studies, greater difficulty or faster movements were more appealing to  
540 naïve observers (Calvo-Merino et al., 2008; E. S. Cross, Kirsch, Ticini, & Schütz-Bosbach, 2011).  
541 These findings correspond to the lower aesthetic and smoothness rankings we found for the  
542 Fast condition (lower ranking of aesthetic proficiency and smoothness indicated greater  
543 excellence). However, we found that aesthetic and smoothness rankings were highest for the

544 Slow-bal condition, the more difficult of the conditions. The expertise of these observers did not  
545 rank balance itself with positive aesthetics. It is likely, they perceived technical problems in the  
546 performers' achievement of that condition.

547 Sato et al. (Sato et al., 2014) investigated the relationship of aesthetic competence to  
548 variability of amplitude, velocity and shape in hip hop dance. Three groups of dancers with  
549 differing skill levels performed the wave. Similar to this study, motion capture stick figures were  
550 rated by experienced judges. Aesthetic judgement discriminated successfully between experts,  
551 non-expert, and novice dancers and correlated highly with smoothness propagation of the wave.  
552 Components of aesthetic technical proficiency include control, accuracy, and fluidity. Therefore,  
553 it is possible that the movement smoothness is a subset of aesthetic technical proficiency,  
554 explaining the high correlation ( $r=0.817$ ) between the two parameters in our analysis.

555 There were also correlations between smoothness rankings and all variables with the  
556 exception of pelvis-hip angle-angle MSD. Again, the highest correlation was to PCA. Dancers'  
557 training focuses on timing and the dynamic quality of movement. Therefore, the observers, all  
558 trained dancers, may have been particularly attuned to the smoothness perception parameter  
559 as it relates to fluidity.

560

#### 561 *Three-D pelvis-hip angle-angle and toe displacement variability*

562 Angle-angle MSD analyses demonstrate variability in coordination patterns during 3-D  
563 joint coupling. This variability may decrease or increase with expertise depending on the task,  
564 offering flexibility to achieve certain goals (Wagner et al., 2012; C. Wilson, Simpson, van  
565 Emmerik, & Hamill, 2008).

566

567 In dance, the aesthetic shape and timing goals may dictate the coordination patterns.  
568 Researchers have reported more stable joint coordination in dancers compared to non-dancers  
569 during a rhythmic coordination task (Kiefer et al., 2011). Greater variability in pelvic motion in  
570 the *développé arabesque*, measured by the coefficient of variability (CV), differentiated between  
571 intermediate and expert dancers in all three planes (Bronner, 2012). The greatest variability was  
572 found in intermediate dancers in the transverse plane. Similar differences for end segment 3-D  
573 toe and finger CV differentiated skill level in the same study. Other dance researchers reported  
574 that CV was able to distinguish between experts and novice hip hop dancers in several  
575 kinematic measures (Sato et al., 2014). Both pelvis-hip angle-angle and 3-D toe MSD findings  
576 in this study were similarly able to differentiate differences between skill in this study.

577 The effect that altered speed and balance constraints have on angle-angle variability is

578 less clear. One study comparing pelvis-trunk coordination and variability in walking and running  
579 found no changes in variability due to speed (Seay, Van Emmerik, & Hamill, 2011). In this study  
580 only 3-D toe MSD distinguished differences between conditions. Pelvis-hip control of the center  
581 of mass may be a critical control parameter, particularly when the participant must stand on one  
582 limb. This may explain our finding of no differences between conditions in pelvis-hip angle-angle  
583 MSD.

584

#### 585 *Principal component analysis*

586 PCA is a technique which reduces complex data sets into smaller set of principal  
587 components which are capable of reproducing the original movement the as a linear  
588 superposition of these modes and hence is an efficient data compression method. The  
589 technique also has the effect of associating noise in the motion with components which add little  
590 variance and hence can often be eliminated from the analysis.. We found that our more skilled  
591 EXP dancers demonstrated lower dimensional components when compared to the INT dancers.  
592 Previously, a different intra-limb organizational strategy was found in the temporal kinematics of  
593 the *développé arabesque* in EXP compared to INT dancers (Bronner, 2012). This difference  
594 may be reflected in the lower number of PCA nodes seen here in the EXP group.

595 Differences due to skill or practice have been reported by other researchers (Ko, Challis,  
596 & Newell, 2003). In 2-D analyses, these researchers reported a shift to lower dimensional  
597 components with learning, represented by two principal components (Ko et al., 2003). In a 3-D  
598 learning study, Hong and Newell reported no change in the number of three principal  
599 components that explained 90% of the variance (Hong & Newell, 2006). However, the  
600 movement was a relatively constrained one on a ski-simulator. In a simple 3-D pointing  
601 movement with an accuracy constraint, researchers reported more than 95% of the variance  
602 was included in one principal component, representing ten joint angles from shoulder to wrist  
603 (Tseng, Scholz, Schoner, & Hotchkiss, 2003). Using a 32 marker set and motion capture,  
604 Hollands et al. (Hollands et al., 2004) reported that only a small number of principal components  
605 were sufficient to describe a 15s movement phrase performed by two professional dancers.  
606 Nine modes represented the dataset, with 82% of the variance represented in the first three  
607 PCAs. However, the movement phrase was not described nor was any difference found  
608 between the two dancers.

609 In this study, dance skill (e.g. group) had a direct effect on the number of active modes  
610 of coordination. Given the complexity of the *développé arabesque* with gesture and stance  
611 limbs, requiring changes in stability, balance and speed, results demonstrated a surprisingly low

612 dimensionality, ranging from four to seven dimensions in EXP and INT dancers respectively.  
613 The Slow-bal condition in EXP dancers was primarily reflected in the 5<sup>th</sup> component, while the  
614 Fast condition was reflected in the 3<sup>rd</sup> and 4<sup>th</sup> components. In contrast in INT dancers, Slow-flat  
615 and Slow-bal were reflected in the higher 5<sup>th</sup>, 6<sup>th</sup>, and 7<sup>th</sup> components while the Fast condition  
616 was primarily reflected in the 5<sup>th</sup> and 6<sup>th</sup> components. Unfortunately, there is no standard way to  
617 analyze or report PCA, therefore it is not possible to directly compare our results to those  
618 previously conducted on dance-related movements.

619 Singular value decomposition (SVD) is similar to PCA in pairing a large number of  
620 features into a smaller subset of major movement structures (Land, Volchenkov, Blasing, &  
621 Schack, 2013; Volchenkov & Blasing, 2013; Volchenkov, Blasing, & Schack, 2014). This  
622 method was able to discern the level of movement expertise in both ballet dancers and golfers.

623 Our results found PCA was also able to discriminate between conditions, with Fast and  
624 Slow-flat demonstrating lower dimensionality than Slow-bal. In contrast, using accelerometry,  
625 PCA was not able to differentiate between conditions in walking at slow, preferred, and fast  
626 speeds (Kavanagh, 2009).

627

#### 628 *Dimensionless jerk*

629 We employed the dimensionless measure of jerk to eliminate differences between the  
630 conditions due to movement duration or extent (Hogan & Sternad, 2009). We observed an  
631 inverted horseshoe in hip and toe jerk histograms for both groups, with the Fast condition  
632 reflecting the greatest smoothness (lower jerk) and Slow-bal condition reflecting the least  
633 smoothness (higher jerk).

634 Minimal jerk theory was initially proposed to explain planning of hand movements in  
635 space. It assumed that movement is based on a kinematic endpoint path trajectory, predicting  
636 straight line paths and bell-shaped velocity curves with a dynamic optimization criterion to  
637 maximize smoothness (Flash & Hogan, 1985). The majority of jerk research has focused on arm  
638 movements based on the endpoint path trajectory. Alternatively, to explain subsequent  
639 observations of the linear relationship of joint velocities when joints move in a coordinated way  
640 and trajectories that are not necessarily straight lines, an optimization-based minimum angular  
641 jerk model was proposed (Friedman & Flash, 2009). Subsequent comparison of this model  
642 using a two-joint index finger grasping movement to other optimization models reported that  
643 the best fit was the angular jerk model.

644 Researchers have demonstrated a decrease in jerk metrics with training or expertise  
645 (Hreljac, 1993, 2000; Schneider & Zernicke, 1989) and increased jerk metrics with increased

646 gait speed when comparing walking and running (Hreljac, 2000). However, none of these  
647 studies utilized dimensionless jerk. As described by Hogan and Sternad (Hogan & Sternad,  
648 2009), the dimensionless jerk measure indicates the number of velocity fluctuations but is  
649 independent of movement duration.

650         Due to the computational complexity of performing a single limb balance while moving  
651 the leg (and torso) at various speeds, durations, and balance constraints, we chose to  
652 investigate dimensionless minimal jerk optimization for both endpoint and angular jerk variables  
653 of the gesture limb. Our results found that both angular and endpoint jerk metrics were sensitive  
654 discriminators between conditions (tempo and balance), but not to discriminate differences in  
655 expertise (group) in this experimental paradigm. Recently, a novel measure for quantifying  
656 movement smoothness, *spectral arc-length* metric, has been proposed to overcome  
657 shortcomings in existing metrics (Balasubramanian, Melendez-Calderon, & Burdet, 2012). This  
658 metric warrants further investigation.

659         Interestingly, the Fast condition revealed **lower rankings in both aesthetic proficiency and**  
660 **smoothness, fewer principle components, lower 3-D toe MSD, and lower jerk.** Although we  
661 manipulated the arabesque sequence with speed and balance constraints, the Fast condition  
662 was not performed at a maximal speed but was metronome controlled. The Fast condition may  
663 have minimized demand on pelvis-hip coordination with subsequent reduction in 3-D toe MSD  
664 due to diminished time in single limb weight bearing. Increased tempo may also have resulted in  
665 reduced sub-movements and lower jerk.

666

#### 667 *Modeling rankings and movement metrics*

668         For aesthetic rankings, model 2 received the least AICc value, indicating that this was  
669 the most parsimonious model for the data. Model 2 modeled aesthetic ranking on the PCA  
670 predictor variable. For smoothness rankings, model 2 again received the least AICc value,  
671 signifying the best fitting model for the data (supplemental data).

672         AIC tells us what variables are important and which are not in establishing a model. If a  
673 variable appears in a model that has a higher AICc score compared to a model that does not  
674 contain that variable, then that variable can be ignored. In the case of both aesthetic and  
675 smoothness rankings, the model with the least AICc value, PCA, corresponded with the highest  
676 correlation values.

677         PCA, which permits the organization of large data sets into simpler groupings, may  
678 reflect how the brain organizes huge amounts of sensory input into chunks (Chen, Penhune, &  
679 Zatorre, 2008; Janata & Grafton, 2003), or, in the case of dance, what is known as phrases.

680 Chunking is thought to be the way in which the brain combines sensory-motor elements into  
681 integrated units of behavior during motor learning. Chunking, in a dynamic process, emerges  
682 spontaneously: as we learn to read, we focus on individual letters and then quickly combine  
683 them into words, leading to groups of words and then whole sentences. A similar process is  
684 thought to occur in both music and dance: we begin with notes or steps, which then become  
685 chunked into short phrases or elemental components which can be linearly, or non-linearly,  
686 combined to recreate a representation of the original experience whilst retaining minimal  
687 information. Sequences become organized into fewer but larger chunks, decreasing the need  
688 for cognitive control with a shift to other neural areas such as those related to motor execution  
689 and ultimately, with expertise, automaticity (Sakai, Hikosaka, & Nakamura, 2004).

690 Orgs et al. (Orgs et al., 2013) suggested a hierarchical model of aesthetic perception of  
691 dance movement: postures, movements, and the larger units of phrases. They suggest that  
692 observer experience may affect how observers weight these hierarchical levels, with dance  
693 experts focusing more on phrasing or larger chunks. Similarly, Bläsing (Blasing, 2014) reported  
694 dance expertise reduced perceived segment boundaries, with, subsequently, longer phrases. In  
695 competitive diving, PCA was applied to kinematic data to predict judges' technical scores,  
696 reporting a high correlation between predicted and actual scores (Young & Reinkensmeyer,  
697 2014). We ask, are the judges extracting fundamental patterns of coordination that reflect these  
698 PCA results?

699 Various motor control theories have attempted to explain how we organize the  
700 complexity of movement with its multiple degrees of freedom. Just as we may use a  
701 minimization cost function of some sort to perform a motor act, the brain may seek to organize  
702 what it perceives to be the simplest mode. Similarly, aesthetic perception may utilize chunking  
703 to assess complex movement. PCA may provide an organizational structure of pattern  
704 recognition to explain this phenomenon. PCA can reveal hidden structure within a complex data  
705 set while simultaneously filtering out noise. The efficiency of smooth movement, minimization of  
706 effort, and clear lines found in the expert dancer were reflected in lower PCA components.

707

### 708 *Limitations*

709 Perhaps ranking was not the optimal metric for aesthetic or smoothness perception. In  
710 the future, we will investigate the effectiveness of Likert scales for multiple components of  
711 aesthetic perception (e.g. both cognitive technical judgement and valience) that observers can  
712 apply to each dancer trial separately. This does not require them to hold in their memory how  
713 the other dancers performed within a given condition.

714 No movement kinetics were included in our models or analyses. Given the important  
715 contribution of dynamics to the quality of dance movement, future investigation will investigate  
716 whether kinematics and/or kinetic metrics are preferred determinants of aesthetic perception.

717

718 *Conclusion*

719 Our examination of a number of biomechanical metrics in a complex dance sequence  
720 with shape, timing, and balance constraints found that PCA best captured the differences due to  
721 expertise and condition. Further comparison between these biomechanical metrics and  
722 movement aesthetic rankings found that PCA provided the most parsimonious model to explain  
723 these observer rankings. If the grace of a dancer is a component reflected in aesthetic  
724 perception, it was not well captured quantitatively by jerk metrics. Perhaps the way our brain  
725 perceives and the way we view movement is that which simplifies the movement into the fewest  
726 organizational groupings; in this case, PCA. A movement with a low PCA dimensionality is  
727 highly constrained and possesses significantly fewer generalized degrees of freedom than joint  
728 variables. The experienced dancers revealed lower PCA dimensionality, and it was these  
729 dancers that were most ranked as most aesthetically proficient. This suggests that reduction of  
730 redundant information, a simplistic dimensionality, may be an important part of observer  
731 perception. Our model of the biological determinant of aesthetics suggests that the brain is  
732 tuned to value movement grace, clarity, fluidity, and efficiency of intent, that is found in the  
733 beauty of dance.

734 In a study employing linear and nonlinear metrics to analyze a complex movement, we  
735 found that the nonlinear PCA was the most promising tool for the quantification of this art form.  
736 Further study of dance biomechanics using PCA may provide insight into motor learning, motor  
737 control, and neuro-aesthetics.

738

739 **Acknowledgments**

740 We thank the participating dancers and other volunteers.

741

742 **Conflict of Interest**

743 The authors declare that they have no conflict of interest.



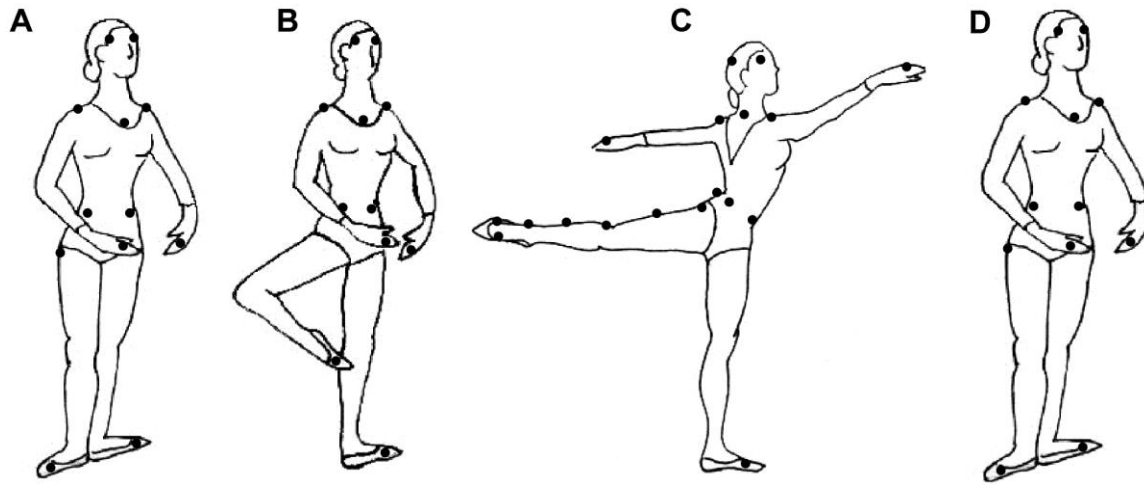
**Table 1. AICc models of aesthetic rankings**

| Model    | Predictors | Parameters     | AICc           | $\Delta$ AICc | F             | df          | p                 |
|----------|------------|----------------|----------------|---------------|---------------|-------------|-------------------|
| 1        | 5          | PCA            | 542.475        | 86.556        | 25.734        | 84,1        | <0.0001           |
|          |            | hip ang jerk   |                |               | 1.736         | 84,1        | 0.191             |
|          |            | toe jerk       |                |               | 1.006         | 84,1        | 0.319             |
|          |            | MSD pelvis-hip |                |               | 0.01          | 84,1        | 0.92              |
|          |            | MSD toe        |                |               | 7.967         | 84,1        | 0.006             |
| <b>2</b> | <b>1</b>   | <b>PCA</b>     | <b>455.919</b> | <b>0</b>      | <b>46.367</b> | <b>88,1</b> | <b>&lt;0.0001</b> |
| 3        | 3          | hip ang jerk   | 572.012        | 116.093       | 1.357         | 87,1        | 0.247             |
|          |            | toe jerk       |                |               | 5.063         | 87,1        | 0.027             |
| 4        | 1          | toe jerk       | 520.174        | 64.255        | 8.743         | 88,1        | 0.004             |
| 5        | 2          | MSD pelvis-hip | 483.974        | 28.055        | 4.451         | 87,1        | 0.038             |
|          |            | MSD toe        |                |               | 10.978        | 87,1        | 0.001             |
| 6        | 1          | MSD toe        | 485.193        | 29.274        | 17.748        | 88,1        | <0.0001           |

745 Abbreviations: AICc, Akaike Information Criteria corrected;  $\Delta$ AICc, change in AIC; PCA,  
746 principal component analysis; ang, angular; MSD, mean standard deviation.

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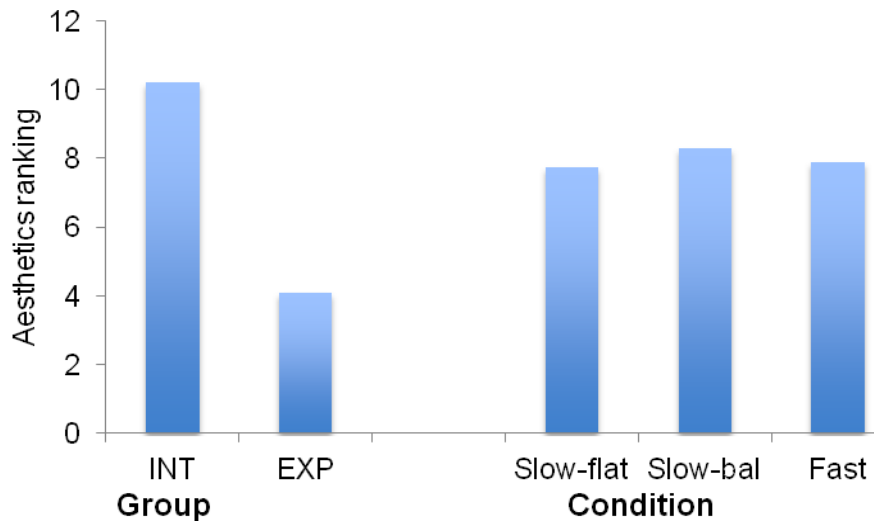
752 Fig. 1 Arabesque sequence for the Slow-flat and Fast conditions: A) First position, B) Passé,

753 C) Arabesque, D) First position. In the Slow-bal condition, the dancers rise onto their forefoot

754 during the arabesque and briefly holds it before returning to first position.

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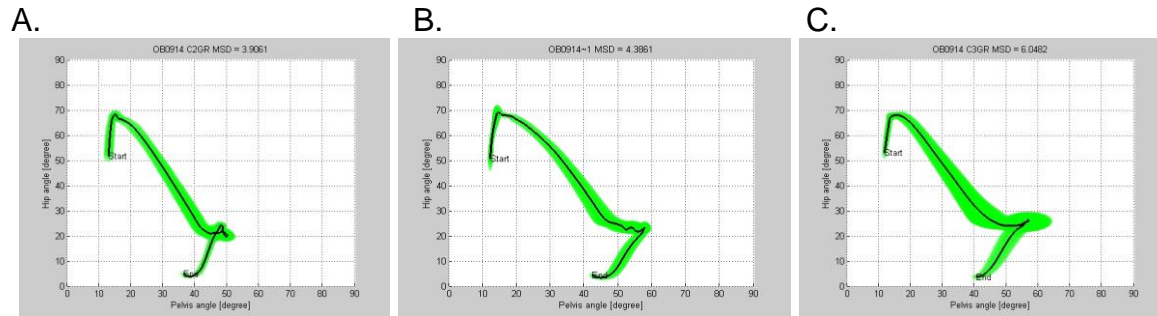
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758 Fig. 2 Aesthetic proficiency ranking. Median for Group and Condition. Note: lower ranking  
759 denotes greater aesthetic excellence.

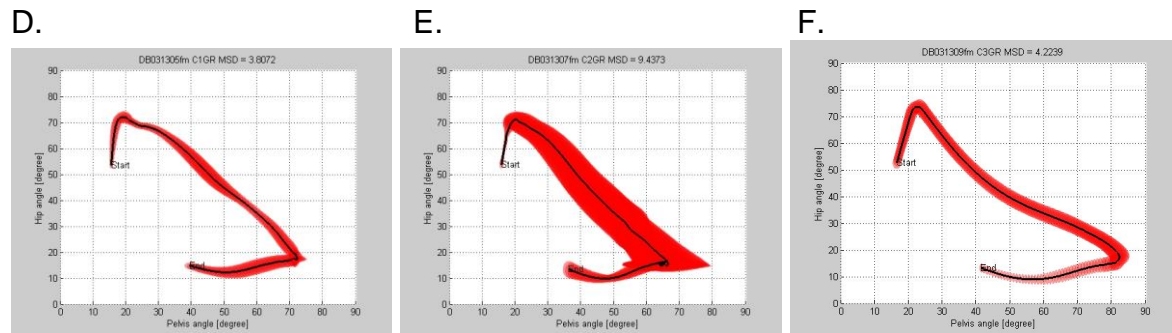
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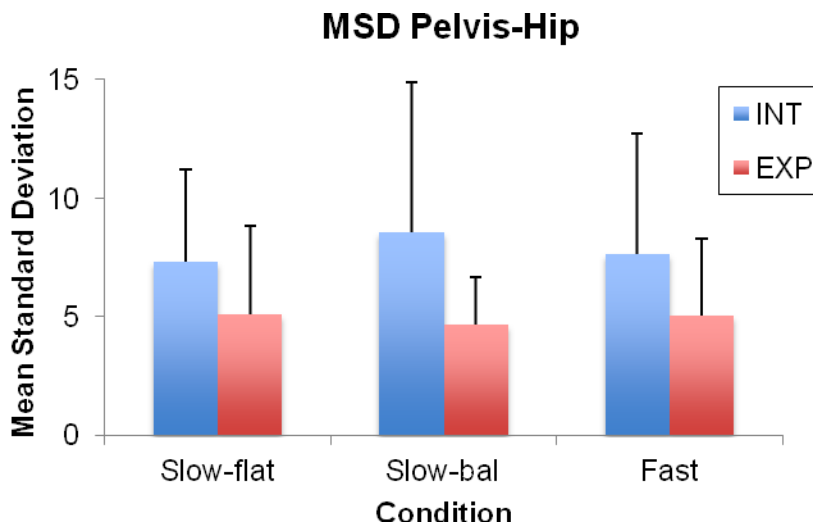


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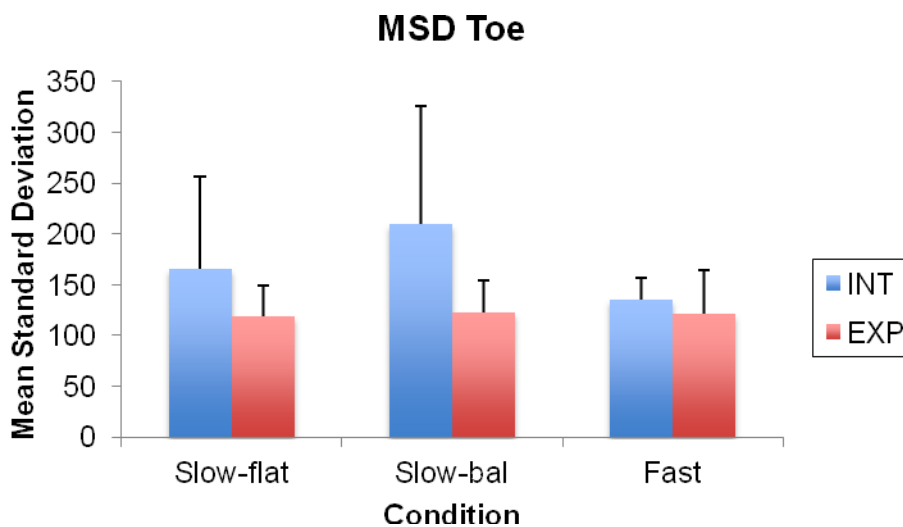
769 Fig. 3 Mean standard deviation (MSD) 3-D pelvis-hip angle-angle plots of representative  
770 subjects. The pelvis is on the x-axis and hip is on the y-axis, the EXP subject is seen in green  
771 and INT subject is in red. A-C. The trial was decomposed into its constituent excursions (six per  
772 trial). On each plot is a line which represents the mean of the excursions together with an  
773 envelope which indicates  $\pm 1$  standard deviation of the excursion trajectories. The colour of the  
774 envelope is red for the INT and green for the EXP dancer. A-C. Representative EXP subject  
775 performing six excursions of the three conditions: A) Slow-flat, B) Slow-bal, and C) Fast. D-F.  
776 Representative INT subject performing six excursions of the three conditions: D) Slow-flat, E)  
777 Slow-bal, and F) Fast.

778  
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781 A.



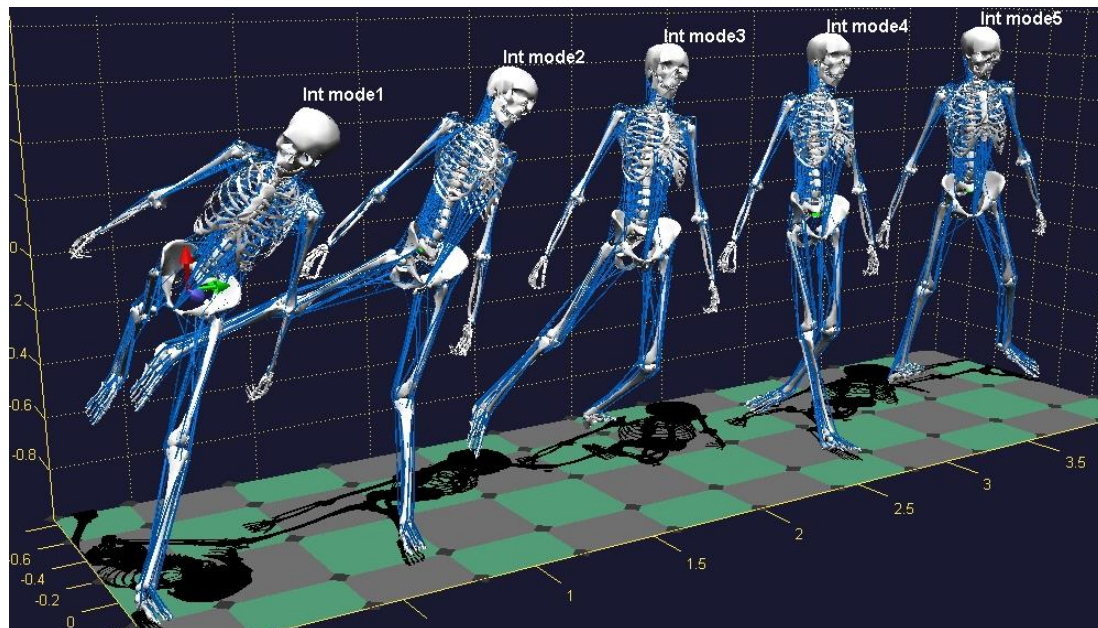
782  
783 B.



784  
785 Fig. 4 Mean standard deviation (MSD) (SD) for 3-D segmental coordination. A) 3-D pelvis-hip  
786 angle-angle; and B) 3-D toe displacement (INT group blue, EXP group red).  
787

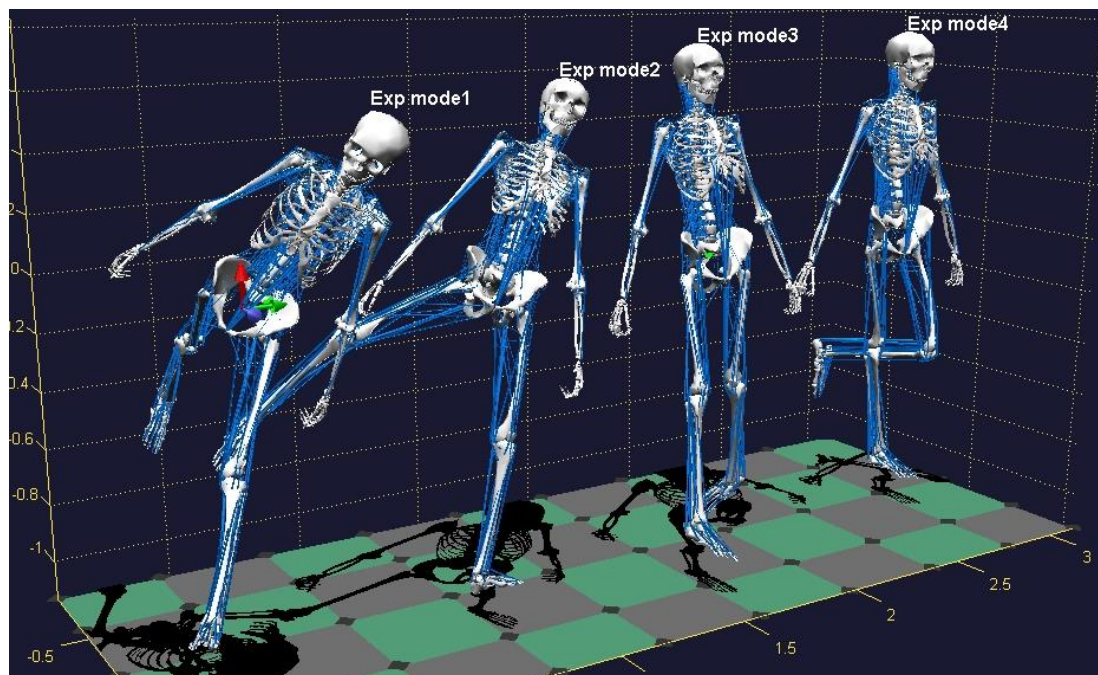
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A.



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B.



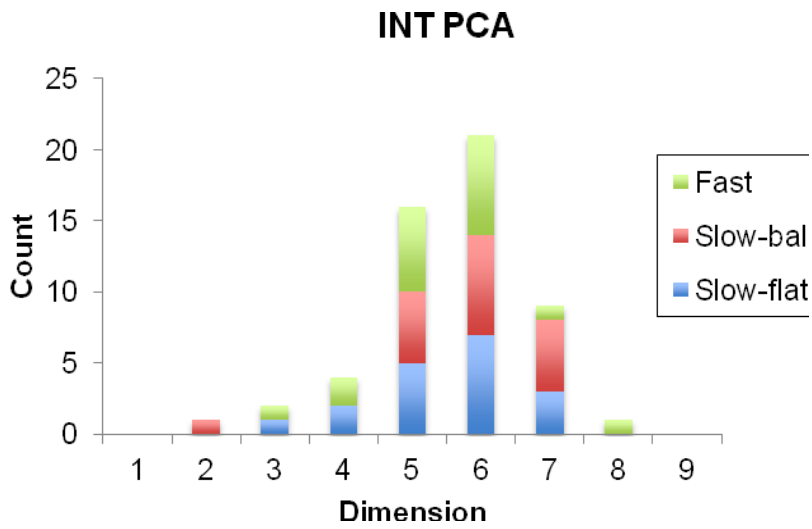
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Fig. 5 Principal components. A) Examples of the five modes which accounted for 98% of the variability of the motion of an INT dancer. B) Examples of the four modes which accounted for 98% of the variability of the motion of an EXP dancer.

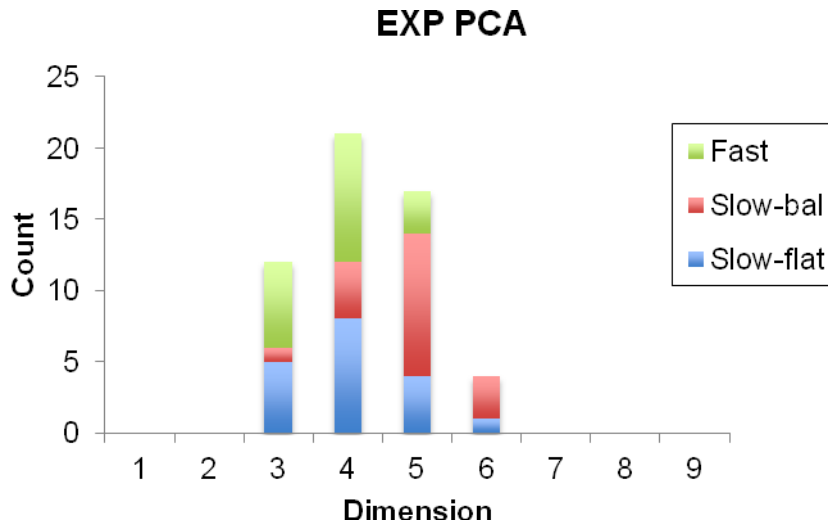
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801 A.



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805 Fig. 6 Principal component analysis. A) Mean dimensionality of the state manifold for the INT

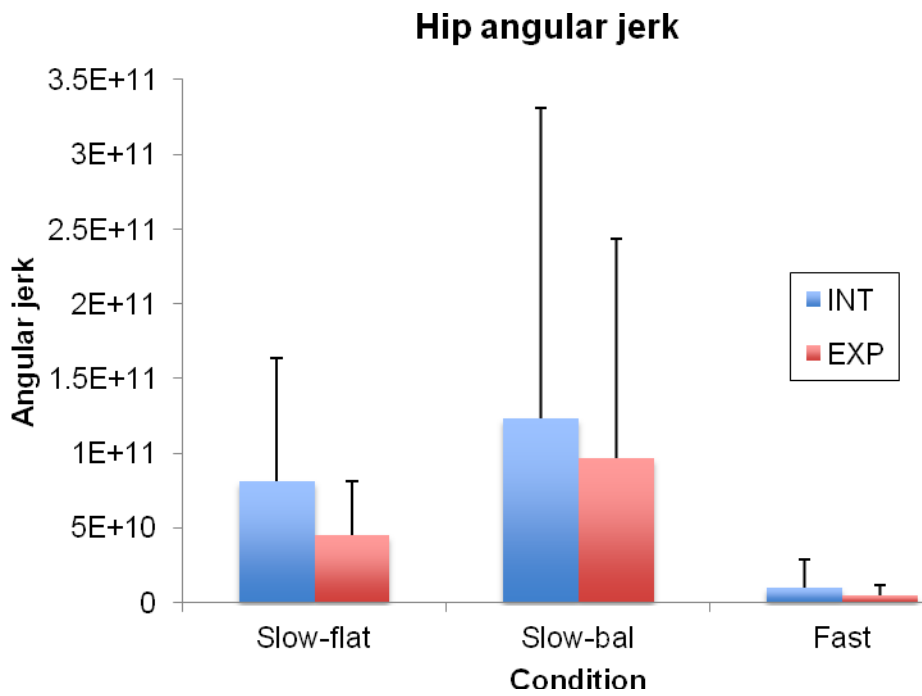
806 group; B) Mean dimension for the EXP group (Blue is Slow-flat, Red is Slow-bal, and Green is

807 Fast condition).

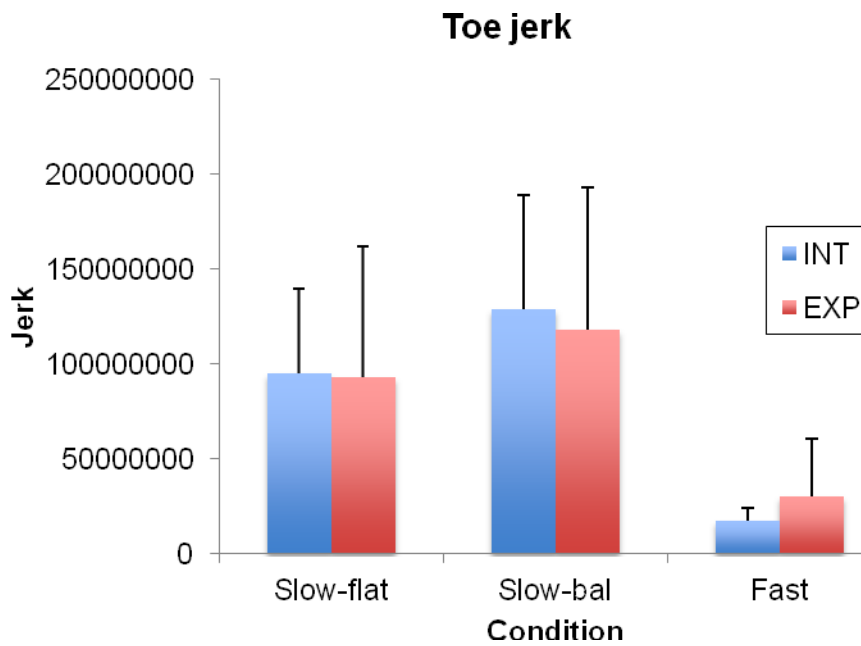
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816 Fig. 7 Mean (SD) dimensionless jerk. A) Sagittal plane gesture hip angular jerk; B) 3-D gesture  
817 toe jerk (INT group blue, EXP group red).

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